SELECTIVE GROWTH OF THERMO-RESPONSIVE POLYMER BRUSHES
THROUGH ORTHOGONAL SELF-ASSEMBLY

by

ABUL BASHAR MOHAMMAD GIASUDDIN
(Under the Direction of Jason Locklin)

ABSTRACT

In this work, thermally responsive poly(N-isopropyl acrylamide) or p(NIPAM) brushes were successfully grafted to multi-component surfaces with chemical selectivity. A catechol based photo-initiator was synthesized and selectively assembled on the surface prior to polymerization. Orthogonal formation of both monolayers and surface selective polymer brushes were confirmed by FTIR. Thick and homogeneous growth of pNIPAM polymer brushes selectively on TiO$_2$ surfaces with dual SiO$_2$-TiO$_2$, was observed using SEM and optical microscopy. Controlled growth of pNIPAM brushes was possible using both different monomer concentrations and photo-irradiation time. Thickest brushes were achieved at saturation concentration of monomer (87% w/w) in solvent and a linear growth in polymer brush thickness formation was observed up to 20 hours of irradiation. The thermal responsive behavior of pNIPAM brushes was confirmed using static contact angle below and above the LCST (Lower Critical Solution Temperature) of pNIPAM. Swelling studies were also performed to estimate the water uptake and release from brush layers below and above LCST.

INDEX WORDS: polymer brushes; pNIPAM; orthogonal self-assembly
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DEDICATION

I would like to dedicate this thesis work to my mother
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CHAPTER 1
BACKGROUND AND LITERATURE REVIEW

Polymer brush definition

Polymer brushes first gained attention in the scientific community in the 1950s, after the discovery that flocculation could be prevented by grafting polymer molecules to colloidal particles (1). In the early 1990s, several groups performed detailed studies on polymer brushes and helped to create an increased awareness of these types of structures (2). Since then, polymer brushes have become an area of great attention. Polymer brushes can be defined as an array of macromolecular chain ends that are covalently tethered to a surface with a density high enough to alter the unperturbed solution dimensions of the chains (3).

The quantitative characterization of a polymer brush can be expressed as the reduced tethered density ($\Sigma$); $\Sigma = \sigma \pi R_g^2$, where $R_g$ is radius of gyration of a tethered chain at specific experimental conditions of solvent and temperature and $\sigma$ is the grafting density. Grafting density is determined by $\sigma = \rho h N_A / M_n$; where $h$ is brush thickness; $\rho$, bulk density of the polymer brush composition; $N_A$ is Avogadro’s number; and $M_n$ is the number average molecular weight (1).
Figure 1. Depiction of mushroom, crossover, and brush regimes of grafted polymer thin films in relation to brush thickness (h) and reduced tethering density (Σ).

Reduced tethered density (Σ) is physically interpreted as the number of chains that occupy an area that a free nonoverlapping polymer chain would normally fill under the same experimental conditions (1). Brush-like character of the grafted film is categorized on the basis of this value (Figure 1).
It is generally recognized that three regimes occur in brush formation:

(1) The “mushroom” or noninteracting regime ($\Sigma < 3.8$),

(2) The crossover regime or mushroom-to-brush transition regime ($3.8 < \Sigma < 6$), and

(3) The highly stretched regime ($\Sigma > 6$).

The transition between single grafted chains and a polymer brush is loosely defined because of the statistical characteristic of grafting and polydispersity of the tethered chains. Resulting fluctuations of the average distance between grafting points can cause an inhomogeneous distribution of across the grafting surface (1).

**Synthesis of polymer brushes**

Synthesis of polymer brushes can be categorized into two groups based on the chemical interaction between polymer and substrate:

1. Physical Sorption and
2. Chemical Sorption.

**Physical Sorption**

Physical Sorption (or Physisorption) is the physically adsorption of polymeric chains on solid surfaces (4-6). Block copolymers provide a general example. In this method, the surface and solvent can be chosen to maximize preferential adsorption of one block to a solid surface while the solvent is chosen to preferentially interact with the other block of a diblock polymer. For example, physisorption of polystyrene-b-
poly(ethylene oxide) (PS-b-PEO) from a toluene solution where the PEO segment is attracted to a mica surface while the PS block is preferentially solvated. More examples of polymer adsorption with only physical interactions are obtained through techniques such as spin coating, spraying, painting etc. Physisorption displays several disadvantages, it is unstable under certain conditions of solvent and temperature, and/or can be displaced by other adsorbents. Figure 2 illustrates the physisorption of polymer on the substrate.

![Figure 2.](image)

**Chemical Sorption**

Chemical Sorption (or Chemisorption) is the covalent attachment of polymer chains at the interface. Due to covalent bond between polymer and substrate, this method enhances the stability of the tethered polymer layers. Covalently attached polymer chains can be synthesized by either the “grafting-to” or “grafting-from” methods.

The scheme in Figure 3 shows both type of chemisorptions “Grafting to” (Figure 3a) and “Grafting from” (Figure 3b).
Grafting To:

The “grafting to” approach is similar to spontaneous adsorption of self-assembled monolayers. In this method a preformed polymer with a reactive end-group is used as the precursor, and the reaction typically occur in liquid phase in order to attach the polymer onto substrates (7). Some of the common reactive functional groups are thiols, silanes, carboxylic acids, and phosphonic acid. One disadvantage of the “grafting to” approach is that it is often difficult to react the end group of a high molecular weight polymer chain with a surface with high yield, the thermodynamics and kinetics of the process also restrict the grafting density. Also, due to chemical compatibility requirements, the available systems with suitable reactive end groups and compatible functional units in the polymer chain are limited in scope.
Figure 3. Schematic illustration of polymer brushes by Chemisorption polymerization, a) “Grafting to” and b) “Grafting from” method.

**Grafting from:**

In the “grafting form” approach, polymer chains are synthesized from a surface through immobilization of a monolayer of surface-initiators followed by in-situ polymerization of selected monomers. This approach is often referred to as surface-initiated polymerization (SIP). The “grafting from” method is significantly more versatile than “grafting to”, and it has been shown that, through SIP, it is possible to assemble densely packed polymer brushes with low polydispersities from a large variety of
monomers in a controllable fashion (8). If there is no free initiator in solution, polymerization occurs exclusively at the surface. Importantly, the grafting density of the polymer chains can be finely tuned by varying the grafting density of the surface initiator (9-10). Because of its versatility, reliability, and control, “grafting from” is attracting significant scientific interest, and is being utilized in application areas such as colloid stabilization, new adhesive materials, protein-resistant bio-mimetic surfaces, chromatographic separation of organic and biomaterials, and organic-inorganic nanocomposites (11-13).

Almost all available polymerization techniques have been applied to graft polymers from substrates. These includes, conventional free radical polymerization, ring opening polymerization, anionic polymerization, cationic polymerization, ring opening methathesis polymerization (ROMP), nitroxide mediated polymerization, atom transfer radical polymerization (ATRP), reversible addition fragmentation chain transfer (RAFT) polymerization (12). One thing that has not been thoroughly investigated is patterning and increased complexity of different chemical functionality spatially distributed in a controlled fashion. Surface-initiated photopolymerization can be an effective and convenient technique to overcome this problem (14-17). Free-radical polymerization by photochemical initiation has distinct advantages, such as ability to build thick brushes, homogeneous distribution of polymer brushes, tolerance for moisture, wide application to a variety of organic functional groups, low cost of operation and potentially reducing negative effects on the bulk polymer (18).
Applications of Polymer Brushes

Polymeric chains as brushes exhibit many distinctive properties compared to polymeric chains in solution. Based on those distinctive properties polymer brushes can be used for multi-dimensional applications. Some of the applications of polymer brushes are highlighted below:

**Stabilization**

Colloidal stability against agglomeration is important in many industrial processes. Stabilization or compatibilization is normally carried out by encapsulating a colloid or particle within a shell of organic polymer; which results in a property mismatch between the composite layers (12). The surface properties of the shell aid or create the desired stabilization. We can get improved properties by compatibilization of colloid or core-shell particles with polymer brushes, as has been demonstrated in the stabilization of latex polymers coated with polymer brush layers (19).

**Surface coatings**

One of the most important fundamental characteristics of surface properties or surface interfaces is adhesion. Surfaces can be functionalized with proteins and cells by physisorption and “grafting to” polymerization methods (20, 21). For example, tissue compatibility has been engineered by creating poly(acrylic acid) polymer brushes on the poly(vinylidene difluoride) surfaces through conversion of the acid-functionalized brush to a fibronectin-coated surface using carbodiimide coupling (22). Polymer brush-coated surfaces also have the ability to provide nonfouling properties. Extracellular proteins strongly adsorb on many surfaces through hydrophobic interactions. Sometimes it is
problematic when specific surface interactions are to be studied, as the co-adsorbing proteins interfere with the desired surface chemistry (23-26).

Super hydrophobic surfaces have been created using patterned polymer brushes and grafted polymer brushes have been used to control wetting (27). By functionalizing a surface with polymer brushes, the morphology can influence the overall performance. The morphology of ultrathin poly-(styrene-b-butadiene-b-styrene) copolymer films deposited on polystyrene brushes has been found to be influenced by grafting density and the DP (degree of polymerization) of the underlying polymer brush layer (28).

Polymer coatings prepared electrochemically tend to have highly desirable properties such as good adhesion and they can be formed on virtually any shaped substrate. However, this process is limited by the final coating thickness, as the electropolymerization is self-limiting and thin brushes are mechanically fragile. Thicker coatings can be produced by sequentially coupling cathodic electropolymerization with another polymerization method. In this way, polymer brushes can be produced on electrically conductive using acrylate-substituted monomers that are functionalized to undergo ATRP and ROMP “grafting from” methodologies (12).
**Separations**

Polymer brushes have been used in chromatographic protein separation and purification (29). Depending on specific solute, solvent, and polymer brush interactions, the quality of separation depends on surface density and chain length of the surface-attached polymer chains, solvent size, and polarity (30). The attachment of polymer brushes to membranes can impact a variety of fluid flow properties. Appropriately functionalized membrane surfaces can improve or enhance separation and resolution through selective adsorption of one component in a mixture (12).

Polymer brushes have also been used as microvalves for the control fluid flow (31). Theoretical investigation of the flow of a good solvent through two closely spaced polymer brush-coated surfaces revealed that the brushes respond to the flow by expanding in response to a shear flow, which causes a decrease in the cross-sectional flow area and a reduction in the flux rate. This pressure-sensitive behavior allows the polymer brush to act as both a sensor and a self-regulating valve. Modeling this behavior revealed that several flow regimes exist and these were found to be dependent on brush height and gap distance between closely spaced parallel plates. It has been found that more sensitive microvalves would result with loosely grafted brushes than with densely grafted brushes (32). Polymer brushes also can be used to create channels which can be opened and closed by controlling solvent properties and pH (33).
Nanofabrication

A combination of “top down” and “bottom up” approaches can be used to pattern and prepare polymer brushes with controlled composition and size of nanoscale features. Researchers at IBM used contact-molding to transfer the pattern from an electron beam-fabricated silicon wafer master to a photopolymer matrix, which contained inimers as one component of the formulation (34). Once casted, the surface-exposed inimers were used as sites for “grafting from” ATRP and nitroxide living free radical polymerization chemistries to produce well controlled polymer brushes with styrene, methyl methacrylate, and hydroxyethyl methacrylate. Through this process, less than 60 could be replicated, with thicknesses ranging from 10 to 143 nm on both flat and nanopatterned surfaces (35).

Surfaces for Electronics

Polymer brushes have been used to make both insulating and conducting surfaces. One of the applications of polymer bruses is as a template in the fabrication of conducting polymer and complementary gold microstructures. Patterned structures can be achieved by acting as the insulating layer during electrodeposition (36). A number of semiconductor processing issues can be improved, by directly attaching polymer brushes to silicon surfaces (37). Conductive polymers can be grafted onto polyethylene and poly(styrenesulfonic acid) films to give conductive poly(thiophene) and poly(ethylenedioxythiophene) surfaces. Chemical sensors based on semiconductive poly(p-phenylene ethynylene) brushes have shown improved stability and displayed
higher emission quantum yields relative to spin-cast films because of reduced aggregation of these systems (38-39).

**Stimuli-responsive polymer brushes**

Polymeric brushes that are responsive to external stimulation are called stimuli-responsive polymer brushes. This kind of coating shows great promise for direct application in areas like sensor systems, drug delivery, microfluidic devices and membrane technology (40-43). The use of external stimuli (e.g., temperature, pH) to effect a change in polymer properties has also been found to be very useful for controlling adhesion on biosurfaces. Among all the stimuli-responsive brushes, particularly thermo-responsive brushes, poly (N-isopropylacrylamide) (pNIPAM) has attracted great attention due to its specific characteristics at Lower Critical Solution Temperature (LCST).

![Figure 4. Schematic illustration of pNIPAM polymer brush behavior below and above the LCST of pNIPAM](image)
pNIPAM undergoes a phase change when taken through its LCST, observed at 32°C. The LCST can be manipulated by changing the N-substituted hydrocarbon chain or through the preparation of copolymers (44).

Figure 5. Water dissociation process of pNIPAm structures at temperatures above the LCST of pNIPAM.

At the LCST, reversible dehydration of the hydrocarbon side chain occurs, causing a collapsed conformation and a change from a hydrophilic to a hydrophobic state, which can result in solubility changes for bulk polymers in solution. This allows for switching of drug reservoirs, microfluidic valves and membrane pores (45-51). Since pNIPAM expels its liquid contents at a temperature near that of the human body, pNIPAM has been investigated by researchers for possible applications in controlled drug
delivery (52). A particular advantage of such polymer based devices is their simple design, which provides the basis for cost-effective fabrication and miniaturization (53).

Orthogonal assembly of molecule

The concept of orthogonal self-assembly was first introduced by Laibinis and Whitesides (54). They reported the selective adsorption of two different adsorbates from a common solution onto a substrate exposing two different materials at its surface. Later orthogonal assembly has also been demonstrated in the presence of two metals (ex. Au and Pt) using isonitriles and thiols (55, 56). The most significant advantage of spontaneous self-assembly over conventional photolithography is in the surface patterning process. In conventional photolithography, different chemical functionality can be incorporated onto a flat substrate routinely using the combination of several patterning and surface activation steps. But in case of three-dimensional and irregularly shaped objects, or when feature size gets smaller and smaller, this technique is not applicable.

Orthogonal functionalization on oxides surfaces can be achieved through either selective deprotonation of a photabile end group or through the oxidation of a homogenous monolayer (57). Selective functionalization on oxides is often found to be difficults with certain anchor groups such as tricholosilanes due to high reactivity, which oligomerize upon exposure to water and can physisorb to almost any surface (58). So selecting specific anchor group on certain oxide surface is currently a major challenge for orthogonal functionalization.
Catechols, are known to chelate a variety of metal oxides via a mononuclear bidentate coordination (59-64). It’s self-assembly on TiO$_2$ and Al$_2$O$_3$ has been exploited in creating both protein resistant surfaces and attaching organic semiconductors to dielectric surfaces (65-67). In our initial studies we have observed that this bidentate coordination cannot occur on SiO$_2$ which means no appreciable monolayers were formed under acid, base, or neutral conditions at room temperature. This characteristic of catechols make it a very suitable anchor group for orthogonal functionalization in TiO$_2$-SiO$_2$ or SiO$_2$-Al$_2$O$_3$ surfaces.
CHAPTER 2

THESIS OBJECTIVE

The research objective of this thesis is to selectively grow thermo-responsive polymer brushes on multi-component surfaces through orthogonal self-assembly. To achieve this, our first aim is to synthesize initiator which can orthogonally form monolayers on multi component surfaces. Once the initiator has been synthesized with surface selectivity, we aim to grow thermo-responsive polymer brushes based on pNIPAM using free-radical polymerization through photo-initiation. We will then investigate the growth of pNIPAM brushes by controlling the monomer concentration and polymerization time. After the growth of pNIPAM brushes, we will perform experiments to characterize the pNIPAM brushes and will analyze some of the basic thermo-responsive behavior of grown polymer brushes in both in-situ and ex-situ above and below LCST.
CHAPTER 3

EXPERIMENTAL DETAILS

Materials

Silicon wafers (orientation (100), native oxide) were purchased from University Wafer. Tetrahydrofuran (THF), purchased from BDH, was distilled from sodium-ketyl. N-isopropylacrylamide (NIPAM) was purchased from TCI and flashed through a basic alumina column to remove inhibitor prior to polymerization. Methanol and dichloromethane (DCM) were purchased from BDH. Dichloromethane (DCM) was distilled over calcium hydride and degassed using freeze-pump-thaw methods. Solvent anhydrous dimethylformamide (DMF) (Drisolv, 99.8% by GC) were purchased from EMD. All other chemicals were purchased from Sigma Aldrich and were used as received.
Synthesis of Photo-initiator

4,4’-Azobis(4-cyanovaleric acid) (2.19 g, 7.8 mmol) was added to thionyl chloride (50 mL) under nitrogen atmosphere. The reaction mixture was refluxed for 15 min in a 100 °C oil bath.

Figure 6. Synthesis of 4,4’-(diazene-1,2-diyl)bis(4-cyano-N-(3,4-dihydroxyphenethyl)pentanamide) (AIBN-catechol)

The hot solution was immersed in an ice bath and cooled to room temperature. Excess thionyl chloride was removed by vacuum evaporation at room temperature to yield a yellow solid. To the crude product was added 25 mL of dry tetrahydrofuran and the solution was bubbled with argon gas one hour to remove dissolved oxygen. In a separate flask, sodium borate decahydrate (2.97 g, 7.8 mmol) was dissolved in 18 MΩ nanopure water (40mL) and also deoxygenated with argon gas for one hour. Dopamine HCl (2.975 g, 15.7 mmol) was added to the water solution, followed by sodium carbonate (2.66 g, 25.11 mmol) and dissolved. The aqueous solution was kept under inert atmosphere and chilled to 0 °C in an ice bath and stirred vigourously. The THF/cyanovaleric acid chloride solution was added dropwise to the chilled solution and
stirred 24 hours. The reaction mixture was acidified to pH 2 using 2M HCl solution and washed three times with 30 mL portions of ethyl acetate. The ethyl acetate layers were collected, dried with MgSO₄, and evaporated to dryness. The crude product was purified by column chromatography using ethyl acetate/hexane (2:1) as the eluent. The product was a yellow solid. 0.923g, 25.6% yield. ¹H NMR (DMSO D₆, 300 MHz) δ (ppm): 8.02 (br s, 1H, OH); 8.00 (br s, 1H, OH); 6.61 (d, 7.9 Hz, 2H, Arom.); 6.57 (s, 2H, Arom.); 6.44 (d, 8.0 Hz, 2H, Arom.); 6.34 (br s, 1H, NH); 3.18 (d, 5.9 Hz, 4H, CH₂NH); 2.54 (d, 7.6 Hz, 4H, CH₂CH₂NH); 2.38-2.24 (m, 8H, CH₂); 1.68 (s, 3H, CH₃); 1.64 (s, 3H CH₃). ¹³C NMR (DMSO D₆, 300 MHz) δ (ppm): 173.29, 145.70, 144.16, 130.81, 119.84, 116.58, 116.11, 72.62, 35.23, 33.94, 32.69, 30.71, 23.60, 21.42.

**TiO₂ Deposition**

Stripes of 1 cm wide TiO₂ were deposited onto clean silicon wafers (University Wafer) by physical vapor deposition from a TiO₂ target using magnetron sputtering (PVD75, Kurt J. Lesker). A tape mask was used to control stripe width. Wafers were rinsed with isopropanol and dried before deposition. The TiO₂ was deposited at 0.5 Å/s using a 50 W power setting and a 5 mTorr capman pressure.

**Orthogonal Self-Assembled Monolayer Formation**

TiO₂ deposited silicon wafer were cut into 1 cm by 2 cm pieces with equivalent amounts of exposed TiO₂ and SiO₂. Then all pieces were rinsed with methanol and N₂ dried. Substrates were Ar plasma cleaned (Harrick Plasma, PDC-32G) on high (18W) for 5 min. The cleaned wafers were placed in methanol with 1 mg/ml catechol photo-initiator
(Scheme 1) and in the dark for 12 hr. The catechol monolayers were rinsed with methanol. Formation of the TiO$_2$ selective monolayer was confirmed by ellipsometry.

**Photoinitiated Polymerization**

NIPAM was dissolved in degassed DCM in a glove box under nitrogen atmosphere. Substrates and dissolved NIPAM were placed in a glass vial and sealed. Vials were placed in a UV light (350 nm) reactor (Rayonet, RPR-600) overnight. NIPAM polymer was grown from the surface and in solution. In order to remove physisorbed polymer, the contents of the vial were soxlet extracted in THF for 12 hrs. Polymer brushes were rinsed with THF and N$_2$ dried.

**Characterization Methods**

Fourier transform-infrared (FT-IR) measurements were taken with a Nicolet model 6700 instrument with a grazing angle attenuated total reflectance accessory (GATR, Harrick Scientific) at 264 scans with 4 cm$^{-1}$ resolution. The film thickness was measured using null ellipsometry performed on a Multiskop (Optrel GbR) with a 632.8 nm He-Ne laser beam as the light source at 70$^\circ$ angle of incidence. Both, $\Delta$ and $\Psi$, were measured and thickness was calculated by integrated specialized software. Several brushes were thicker than the limit allowed by null ellipsometry due to the asymptotic $\Psi$ function. Brushes above this limited were characterized by profilometry using a Dektak 150 stylus profiler. Measurements were taken at 0.1 $\mu$m/sample using a 0.2 $\mu$m tip with a stylus force of 3.00 mg. At least three measurements were taken for each brush, and the
average thickness was recorded. Where applicable, brush thickness was confirmed by null ellipsometry and profilometry.

Spectroscopic ellipsometry (M-2000V, J.A. Woollam Co., Inc.) was used to track the dynamics of swelling. Ex situ measurements were taken at 65°, 70°, and 75° in order to fit the refractive indices and film thicknesses of the dry pNIPAM brush using specialized software provided by the company. Substrates were characterized after each film addition, reducing the number of variables required to fit the model over the spectral range, 380-1000 nm. In situ measurements were performed in a flow cell at a 60° angle of incidence. The Δ and Ψ values were monitored as the temperature of the water within the cell was cycled between 25 °C and 50 °C.

Contact angles of water drops were measured (Kruss, DSA100) using a white light source and a CCD camera. The syringe is fixed in an automatic dispenser that controls the size and deposition of the droplet. The contour of a sessile drop is analyzed and fitted to the Young-Laplace equation using a contour tracing algorithm that distinguishes the drop from the surface. For statistical purposes, at least three drops were measured on each sample. The reported contact angles are the average of these measurements.

Scanning electron microscopy-energy dispersive spectroscopy (SEM-EDS) (FEI Inspect F FEG-SEM equipped with EDAX EDS) was used to image the orthogonal nature of the self assembly. SEM was controlled by xTm (ver. 4.1.0.1910). The sample
was placed on the sample holder with double sided adhesive conductive carbon tape and was ready for analysis. The sample was set on its side to image the polymer brush from the side.
CHAPTER 4
RESULT AND DISCUSSION

In our study, we first synthesized AIBN-catechol photo-initiator specifically selected for orthogonal monolayer formation on TiO₂. Then orthogonal self-assembled monolayers (SAMs) were then formed on the TiO₂ part of SiO₂-TiO₂ dual surfaces using the catechol based initiator. Once the SAMs were formed on selective parts of the substances, pNIPAM brushes were grown using photo-initiated free radical polymerization. A schematic Illustration of the total process can be seen Figure 7.

Figure 7. Schematic of orthogonal monolayer and polymer brush formation on SiO₂ - TiO₂ dual surfaces.
Orthogonal Self Assembled Monolayers (SAMs) were formed using 1 mg/ml AIBN-catechol based initiator (the structure of which is shown on figure 7) in methanol solution overnight, which generated a 2 nm homogeneous SAM selectively on TiO$_2$. Ellipsometric data confirmed the absence of monolayer on the SiO$_2$. Thermo-responsive pNIPAM polymer brushes were grown from TiO$_2$ surface by photo-irradiating SAMs of AIBN-catechol photo-initiator in an O$_2$ free environment. In presence of UV (350nm) the AIBN-catechol generates radicals, which initiates the growth pNIPAM brushes.
Surface Characterization of pNIPAM Polymer Brushes

FTIR spectra of orthogonal self-assembled monolayer and pNIPAM brush on TiO$_2$ surfaces are demonstrated in Figure 8a and Figure 8b.

Figure 8. FTIR spectra of (a) AIBN-Catechol monolayer and (b) pNIPAM brush on TiO$_2$ surfaces.

Deprotonated, metal co-ordinated stretching of C-O group at 1235 cm$^{-1}$ in Figure 8a confirmed the catechol monolayer formation on TiO$_2$ (60). In Figure 8b, the absorption peak at 3285 cm$^{-1}$ and 1540 cm$^{-1}$ indicate the stretching of the secondary amide group. Peak at 2960 cm$^{-1}$ is due to asymmetric stretching of -CH$_3$ group and 1460 cm$^{-1}$ is due to asymmetric bending of -CH$_3$ group. Strong absorption peak at 1650 cm$^{-1}$ is
due to secondary amide C-O stretching. Stretch for two –CH$_3$ groups of the isopropyl functionality can be seen peak at 1369 cm$^{-1}$ and 1389 cm$^{-1}$. Observed bending and stretches confirmed the formation of covalent bond of pNIPAM brush (68, 69).

Figure 9. SEM images of selective growth of pNIPAM brush on TiO$_2$ of SiO$_2$-TiO$_2$ surfaces. Polymerization time was 24 hours and saturated concentration of NIPAM (87% (w/w)) monomer was used. a) Top view of pNIPAM brush, and b) Cross sectional view of pNIPAM brush.

Figure 9 shows a representative SEM image of the dual surface with the selective growth of pNIPAM from the TiO$_2$ surface. Figure 9a clearly shows the NIPAM polymer brush growth on TiO$_2$ with no coating observed on SiO$_2$, which confirm the
homogeneous orthogonal growth of pNIPAM from catechol based initiator. Figure 9b shows the cross sectional view of a pNIPAM polymer brush with a thickness of 1.2 μm.

**Controlled Growth of pNIPAM Brushes**

The thickness of pNIPAM brushes can be controlled by varying the monomer concentration. Various monomer concentrations of NIPAM in DCM were subjected to the same polymerization conditions. The saturation limit of NIPAM in DCM was found to be 87% w/w. Different concentrations of NIPAM monomer were used ranging from 50 to 85% w/w (Table 1) for polymerization at a fixed time of 24 hours.

**Table 1.** Surface selective pNIPAM brush thickness at different concentrations of monomer (pNIPAM) in DCM grown after 24 hours of UV λ = 350 nm irradiation

<table>
<thead>
<tr>
<th>wt% (N-isopropylacrylamide)</th>
<th>Thickness (nm)</th>
<th>Error ± (nm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>50</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>65</td>
<td>107</td>
<td>6</td>
</tr>
<tr>
<td>70</td>
<td>185</td>
<td>12</td>
</tr>
<tr>
<td>75</td>
<td>270</td>
<td>30</td>
</tr>
<tr>
<td>80</td>
<td>635</td>
<td>45</td>
</tr>
<tr>
<td>85</td>
<td>915</td>
<td>150</td>
</tr>
</tbody>
</table>
Brush thickness relative to monomer concentration is demonstrated in Figure 10. Concentrations below 50% w/w resulted in no polymer growth from the surface or in solution. The polymerization reaction from the surface in our case was limited by the amount of initiator and mass transport of monomer to the initiator. AIBN is a stable thermal initiator with a half-life on the order of hours.

Figure 10. Thermo-responsive pNIPAM brushes on TiO$_2$ surfaces grown at different initial NIPAM monomer concentrations, % (w/w) in DCM solvent and UV (350nm) irradiated polymerized for 24 hours. Dashed line (--) is to guide the eye.
The longer the half-life, the longer the radical persists which increases the time frame in which a single initiator can start a polymerization once in contact with a monomer unit. In our case, the mobility of the monomer is limited by the diffusion rate through the solution. With low initiator concentrations and slow diffusion, the rate of initiation is minimal at lower monomer concentrations. At higher weight fractions, we were able to grow pNIPAM brushes a various thicknesses depending on the concentration of monomer (Figure 10). Brush thickness is reproducible for each weight fraction indicating a reproducible non-linear relationship between thickness and monomer concentration. The thickest brush of 1.2 µm was achieved at the saturation limit of NIPAM in DCM.
Figure 11. Polymerization time and brush thickness exhibiting a linear relationship with 65% w/w monomer in DCM. Dashed line (--) is to guide the eye.

Brush thickness was also characterized with respect to time at a constant NIPAM concentration of 65% w/w (Figure 11). A linear relationship in polymerization time and brush thickness was observed. The linear relation of photoinitiated polymerization with time proved the continuous generation of radicals which can diffuse through the already grown brush on the surfaces to react with more NIPAM monomer (Table 2).
Table 2. Relationship between dry pNIPAM brush thickness and UV irradiation time at 65% (w/w) N-isopropylacrylamide in DCM

<table>
<thead>
<tr>
<th>Time (min)</th>
<th>Thickness (nm)</th>
<th>Error ±(nm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>45</td>
<td>12</td>
<td>2</td>
</tr>
<tr>
<td>90</td>
<td>17</td>
<td>2</td>
</tr>
<tr>
<td>210</td>
<td>26</td>
<td>6</td>
</tr>
<tr>
<td>420</td>
<td>51</td>
<td>3</td>
</tr>
<tr>
<td>840</td>
<td>80</td>
<td>3</td>
</tr>
<tr>
<td>1080</td>
<td>107</td>
<td>12</td>
</tr>
<tr>
<td>1440</td>
<td>115</td>
<td>8</td>
</tr>
</tbody>
</table>

After 20 hours, the polymerization ceased due to the decay of UV generated radicals and reduction of diffusion of radicals through polymer brush.
Thermally Responsive Behavior of pNIPAM Brushes

Contact angle measurement

Static water contact angle measurements were used to investigate the surface wettabilities before and after the formation of orthogonal monolayers and pNIPAM brushes. The contact angle measurements were taken at room temperature and surfaces were N₂ dried before measurement.

Figure 12. Static water contact angle on SiO₂-TiO₂ surfaces a) Bare surface, b) Orthogonal monolayer grown surface and c) Orthogonal pNIPAM brush grown surface. Contact angles on SiO₂-TiO₂ surfaces were measured after ringing with water and drying by purging N₂.
Figure 12 demonstrates the static contact angle changes due to formation of orthogonal monolayers and pNIPAM brushes on SiO$_2$-TiO$_2$ surfaces. Plasma clean SiO$_2$-TiO$_2$ patterned surface shows no contact angle on either oxide surface (Figure 12a) but once orthogonal self-assembled monolayer formed, the contact angle on TiO$_2$ surface was 30° and 15° on SiO$_2$ (Figure 12b). Contact angle on the pNIPAM brushes on TiO$_2$ surface was observed as 62° (Figure 12c) but on the on SiO$_2$ part of the surface the contact angle remain same as 15 which confirmed the surface selective growth of pNIPAM brushes (70-72).

To understand the surface wettability of the pNIPAM brushes above and below the LCST (32°C), we measured the contact angles at two different temperatures 40°C and 25°C (Figure 13). After soaking the film at 25°C for 20 min and then N$_2$ drying, a value of 62 was obtained indicating a hydrophilic surface. When immersing the substrate into water with temperatures above the LCST (40°C) for 20 min, the contact angle increased to 73°, which indicates the partial hydrophobic behavior of the pNIPAM brushes. At temperature below LCST, pNIPAM chains stay in an extended conformation due to the hydrogen bonding with water and amide group but above LCST, the pNIPAM brushes adopt a more collapsed confirmation due to the breaking of the hydrogen bonds with amide group which made pNIPAM brush more hydrophobic (75).
Figure 13. Transformation of static water contact angles on pNIPAM brushes on SiO$_2$-TiO$_2$ surfaces due to temperature cycling below (25°C) and above (40°C) LSCT. Contact angles were measured on the N$_2$ dried brush after soaking in water for 20 minute at 25°C and 40°C consecutively.

We also investigated the reversible thermo-responsive behavior of pNIPAM brushes. Figure 13 shows the contact angle on NIPAM polymer brush changes from 62 to 73 in below (25°C) and above (40°C) LSCT which was consistent in several temperature cycles.
Swelling Behavior of Orthogonal pNIPAM Brush

Dynamic tracking of pNIPAM swelling was monitored by spectroscopic ellipsometry. Several pNIPAM brushes were grown on a 3 cm by 1.5 cm substrates. Each layer was characterized by spectroscopic ellipsometry using \textit{ex situ} measurements of $\Delta$ and $\Psi$ and known refractive indices for the silicon, silicon oxide, and titanium oxide layers. The polymer film was characterized by fitting the brush thickness, refractive index, and extinction coefficient. The Cauchy model, Eq. 1, was used to fit the refractive index, $n$, while the Urbach equation, Eq. 2, was used to determine the extinction coefficient, $k$,

$$n = A + \frac{B}{2} + \frac{C}{4}$$ \hspace{1cm} (1)

$$k = k_0 e^{D(E - B')}$$ \hspace{1cm} (2)

where $A$, $B$, and $C$ are Cauchy parameters and $k_0$ and $D$ are Urbach parameters. Fitting the above model to the $\Delta$ and $\Psi$ spectra produced an average refractive index of $1.52 \pm 0.03$ and extinction coefficient of $0.04 \pm 0.005$ at a wavelength of 632.8 nm. Most organic film models assume a value of zero for the extinction coefficient indicating no light scattering within the film. For thin NIPAM films, 20-30 nm, fitting the extinction coefficient results in a zero value. Thicker films exhibit non-zero values, which can be attributed to light scattering due to the heterogeneous nature of the film.
In situ tracking of the hydrogel swelling and collapse was performed at an angle of incidence of 60° in a custom flow cell. The substrate was immersed in 18 MΩ H₂O at 25°C for 1 hr to ensure that the polymer brush was intercalated with water. Spectral curves of Δ and Ψ were taken for several minutes prior to flowing in 50°C water followed by a rinse with 25°C water. Flowing in water above the LCST produces a change in Δ and Ψ due to polymer collapse, as shown in figure 14. In tracking mode the spectroscopic ellipsometer takes complete spectral data at each time interval.
Figure 14. Spectroscopic ellipsometry values of delta and psi for NIPAM collapse due to temperature changes. Values are taken from an *in situ* experiment where a NIPAM film is cycled through collapse and swelling by changing solvent temperature from 25°C and 50°C, taken at 0min and 70 min, respectively. Dashed lines represent modeled values of delta and psi from fitted parameters; film thickness, refractive index, and extinction coefficient.
The dynamic data was modeled using equations 1 and 2. Changing the Cauchy and Urbach parameters produces the fits shown in figure 14 for the swollen and collapsed film. The modeled values for thickness, refractive index, and extinction coefficient for each time interval are reported in Figure 15. Injecting water above the LCST produces an immediate response in the polymer as indicated by the drastic decrease in brush thickness from 90 nm to 72 nm at 2 min.

Figure 15. In situ spectroscopic ellipsometry tracking NIPAM collapse due to solvent temperature changes. Thickness, refractive index, and extinction coefficients are derived from modeling delta and psi values. The film collapses when 50°C water is injected at
2 min. Replacing the solvent with 25°C water swells the polymer to the starting thickness after a period of rearrangement.

Substantial changes in the film’s refractive index are also observed. In the dry state the polymer brush has a refractive index of 1.52. The refractive index of the hydrogel resembles that of a polymer-water mixture producing an effective refractive index for the brush layer that is lower than the dry polymer. When the brush collapses, the polymer contracts squeezing water out of the film and the effective refractive index for the layer increases towards that of the dry film. Changes in the extinction coefficient are not observed indicating similar light scattering properties for the swollen and collapsed film. In figure 15, an adjustment factor of 1.3 was used to plot the extinction coefficient on the same scale as refractive index. The extinction coefficient during the dynamic tracking fluctuates within the range reported for the dry film.

Limiting the organic brush model to a single layer provides the effective refractive index for that layer. The layer is actually a mixture of water and polymer each with distinct refractive indices and volume fractions. By applying the Maxwell-Garnett effective medium approximation, Eq. 3,

\[
\frac{n_{\text{eff}}^2 - n_p^2}{n_{\text{eff}}^2 + 2n_p^2} = \Phi_w \frac{n_w^2 - n_p^2}{n_w^2 + 2n_p^2}
\]  

(3)
where $n_p$ and $n_w$ are the refractive indices for pNIPAM and water, $n_{eff}$ is the modeled refractive index profile, and $\Phi_w$ is the water volume fraction within the hydrogel which was computed over the dynamic range, Figure 16. The refractive index of the dry polymer was used for $n_p$ and a value of 1.33 was used for $n_w$. Below the LCST the hydrogel is swollen with a 0.80 water volume fraction. In the collapsed state, above the LCST, the polymer film contains a 0.30 water volume fraction within a smaller volume than the swollen state.

Figure 16. Volume fraction of water in the NIPAM brush as computed by the Maxwell-Garnett effective medium approximation. The dynamic data starts out with a swollen brush at 25°C. Water is released when the film contracts reducing the volume fraction in the thinner collapsed film.
In raising the temperature above the LCST, the hydrogel loses ~70% of water from the swollen volume due to polymer contraction. Using a temperature of 50°C the polymer contracts completely within 25 seconds. Injecting 25°C water at 4.5 min the polymer is taken below the LCST and the film again swells to a 0.80 water volume fraction in ~30 sec. Re-swelling of the pNIPAM involves rearrangement of the polymer brush which is expected to take longer than polymer contraction. For each case, collapse or re-swelling, changes in the film occur rapidly at the experimental temperatures. Fluctuations in the dynamic data after the initial swelling also indicate some rearrangement within the film, as is evident in Figure 15 and 16.
CHAPTER 5
CONCLUSION

This research work has been performed in three logical steps involving the
1. Synthesis of photo initiator for orthogonal self assembly on multi component surfaces,
2. Homogeneous grafting of thermo-responsive polymer brush on the selective surfaces
Initially we have synthesized catechol based photo-initiator and used this initiator to
orthogonally self-assemble onto the TiO$_2$ side of SiO$_2$-TiO$_2$ dual surfaces. After
successful initiator immobilization, we grafted thermo-responsive pNIPAM brush on the
monolayer using UV irradiation, which yielded densely packed polymer layers
selectively on TiO$_2$. Selective growth of thick and homogeneous pNIPAM brush was
confirmed using FTIR and SEM.

The growth of the polymer brush layer was controlled by changing concentration
of monomer in the solvent and polymerization time. The grown pNIPAM brush was
found to have thermo-responsive behavior gaining hydrophobic characteristics above its
LCST. Also this thermo-responsive behavior was found be reversible with many cycles.
Our swelling study showed the volumetric change below and above LCST due to gain
and release of water from polymer brushes.
The result of this research is significant from several points of view. First of all, the surface selective growth of polymer brushes opens the door for nanoscale surface patterning. Secondly, the possibility of targeting functionality on multi-component surfaces is of great utility on irregularly shaped objects or nanoscale systems. Thirdly, the growth of thick and homogenous growth of thermo-responsive polymer brushes are now available to investigate different biomedical applications such as drug delivery. Overall, this research work is a successful representation of the surface selective growth of stimuli-responsive brushes on multi-component surfaces.
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